

1 **Running title:**

2 **A novel artificial endothelial replacement membrane for the treatment of chronic corneal**
3 **edema: A first-in-human trial**

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21 OD, ALM, EG and AL are employees at EyeYon Medical. For the remaining authors none were
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23

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25 Keratoprosthesis; Corneal Edema; Endothelial Keratoplasty; Corneal implantation; EndoArt.

26

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28 The FIH trial was fully funded by EyeYon Medical, a developer of the EndoArt® implant.

29 Abstract

30 Purpose: To report the safety and efficacy results of an artificial lamellar implant for the
31 treatment of chronic corneal edema.

32 Methods: The EndoArt[®] (EyeYon Medical, Ness Ziona, Israel), an artificial endothelial
33 replacement membrane designed to treat corneal edema, was implanted in 24 eyes of 24
34 subjects with low to normal visual potential. We present the safety and efficacy results from a
35 prospective, open-label, single-arm, multi-center study conducted over a 12-month period.

36 Results: No device-related serious adverse events (SAEs) were reported during the follow-up
37 period. The average central corneal thickness (CCT) was reduced from 759 ± 116 μm at baseline
38 to 613 ± 135 μm at the 12-month follow-up. Best corrected distance visual acuity (BCDVA)
39 improved from an average of 1.88 ± 0.79 logMAR pre-operatively to 1.34 ± 0.57 logMAR at the 12-
40 month follow-up. Sixty percent of the subjects gained at least 3 early treatment diabetic
41 retinopathy study (ETDRS) lines at 12 months. In five subjects, the EndoArt[®] was removed due to
42 incomplete attachment, and they eventually underwent corneal transplant. No device-related
43 long-term complications, infections, or inflammations were reported. The implants remained
44 transparent throughout the study.

45 Conclusions: The first-in-human (FIH) results of EndoArt[®] implantation demonstrated the
46 device's potential to treat patients suffering from corneal edema with a favorable safety profile
47 and effective edema reduction in most patients, with no device-related SAE. The EndoArt[®] may
48 offer a viable solution in regions with a shortage of donor corneas and for patients who have
49 rejected human tissue.

50 Introduction

51 Endothelial keratoplasty (EK) is currently the preferred surgical option for treating refractory
52 corneal edema, with Descemet stripping automated endothelial keratoplasty (DSAEK) and
53 Descemet membrane endothelial keratoplasty (DMEK) offering good visual acuity and resolution
54 of corneal edema.¹⁻⁴ However, these surgeries rely on human donor corneas, which are limited
55 in availability and require carefully calibrated processing, transport, and storage conditions. As a
56 result, millions of people with corneal blindness are left without a viable vision restoration
57 solution.⁵⁻⁷ Additionally, EK is associated with reduced endothelial cell counts and graft rejections
58 even when performed by experienced cornea specialists.⁸⁻¹⁰ A comprehensive retrospective
59 analysis of 30,600 eyes from the Intelligent Research in Sight (IRIS) registry investigating visual
60 acuity (VA) outcomes following EK procedures in the United States revealed that approximately
61 30% of the eyes did not achieve any visual improvement at the one-year mark after surgery.
62 Moreover, approximately 15% of patients experience decreased VA when using human tissues.
63 Notably, within this extensive cohort, postoperative re-bubbling and repeat keratoplasties were
64 identified as independent factors associated with poorer VA outcomes.¹¹ The success of human
65 corneal graft transplantation is strongly dependent on the recipient's condition, as comorbidities
66 such as glaucoma, prior trabeculectomy, and anterior chamber intraocular lens (ACIOL) markedly
67 lower graft retention.

68 A synthetic device¹² that can alleviate corneal edema and serve as an alternative to the donor
69 corneal lamella would benefit patients at high risk for human graft rejection and failure.^{13,14} A

70 synthetic device with a long shelf life is also readily available and may offer an additional option
71 in regions with a shortage of human corneas.

72 The notion that a synthetic plate can substitute for the corneal endothelium and attenuate
73 corneal edema came from clinical observations and literature reports of aphakic silicone oil-filled
74 eyes, with silicon in the anterior chamber, after retinal detachment repair surgeries, which
75 exhibited a clear cornea despite a low endothelial cell count, suggesting that the barrier
76 mechanism of the silicone could substitute for the function of the corneal endothelium and
77 attenuate corneal edema. After silicone oil removal, the corneas immediately became
78 edematous, demonstrating the blocking function of the plate and its potential for treating
79 patients with corneal edema.¹⁵⁻¹⁸

80 A possible explanation for the barrier mechanism is that in a steady state, the relation between
81 the inflow and outflow of fluids into and out of the cornea determines its thickness.¹⁹ This
82 process, governed by passive and active mechanisms, a passive barrier formed by a healthy
83 endothelium and epithelium (tight junctions) which passively limit inflow into the cornea and an
84 active process, the endothelial Na-ATPase pumps that pump fluid out of the cornea, in
85 conjunction with tear film evaporation, to a lesser extent. However, when the endothelial cell
86 count decreases, outflow diminishes, leading to a new relationship between inflow and outflow
87 and creating a new steady state characterized by increased stromal water content and
88 subsequent thickening, known as corneal edema.²⁰⁻²³ The EndoArt® implant reinforces the
89 passive barrier, by blocking the central portion of the posterior cornea and reducing inflow into
90 the cornea, thus establishing a new steady state, resulting in a thinner cornea and alleviated

91 corneal edema. The hypothesis suggested that the uncovered peripheral posterior surface of the
92 cornea would facilitate sufficient fluid influx and nutrient transport, ensuring safe corneal
93 physiology without adverse events such as corneal melting or perforation. Furthermore,
94 considering the relatively broad range of corneal thicknesses within which the cornea remains
95 transparent, EndoArt® seeks to reduce corneal thickness to approximately 420-625 µm.²⁴ This
96 range generally signifies a clear and viable cornea. The implant is composed of a transparent,
97 flexible, water-impermeable, biocompatible synthetic material that can seal a part of the inner
98 corneal surface to relieve corneal edema in the absence of a functioning endothelium (EndoArt®,
99 EyeYon Medical, Ness Ziona, Israel). Prior to human testing, EndoArt® was tested and validated
100 in porcine and leporine eyes with induced corneal edema.^{12,25} The synthetic implant provided
101 relief from edema and restored corneal transparency over a 12-month follow-up period, while
102 the control eyes continued to suffer from persistent and severe corneal edema. Additionally,
103 compassionate implantation of the device in subjects who had previously failed multiple corneal
104 transplantations has concluded that implantation of the EndoArt led to rapid corneal
105 deturgescence and CCT restoration, presenting a possible option for patients with chronic
106 corneal edema.²⁶

107 The FIH study, completed in January 2023, focused primarily on evaluating the safety of EndoArt®
108 and refining both the design of the implant and its implantation technique.

109

110 Materials and Methods:

111 A multicenter, international, non-randomized, open-label, prospective trial was conducted in
112 Israel (Soroka Medical Center Beer Sheva, Rambam Medical Center Haifa, Sourasky Medical
113 Center Tel-Aviv, Barzilai Medical Center Ashkelon, and Assuta Medical Center Tel-Aviv), the
114 Netherlands (UMC, Amsterdam), Spain (IMO, Barcelona), Germany (Universitäts-Augenklinik,
115 Heidelberg), and India (LV Prasad Hyderabad), and adhered to the Declaration of Helsinki. The
116 institutional review board of each center approved the study, and subjects who met the eligibility
117 criteria provided informed consent, including consent for the publication of results, before any
118 study-related procedures were performed.

119 The primary safety endpoint was the frequency and severity of adverse events related to the
120 EndoArt® device documented during and up to 12 months after implantation. Adverse events of
121 particular concern include corneal perforation, corneal melting, uncontrolled inflammation, and
122 severe infection. The secondary efficacy endpoints were CCT and BCDVA.

123

124 Subjects:

125 The participants were required to be older than 40, pseudophakic, and have a stable posterior or
126 anterior intraocular lens (IOL) with chronic corneal edema and a minimal CCT of 650 μm . A VA of
127 6/30 (0.70 logMAR) or worse was needed, with better VA recorded in the contralateral eye.
128 Patients were excluded if they had any of the following: BCDVA of 6/30 (0.70 logMAR) or worse
129 in the fellow eye, a history of ocular herpes simplex keratitis, a severely scarred cornea unsuitable
130 for regular EK, irregular posterior cornea, current corneal infection, band keratopathy, limbal
131 stem cell deficiency, clinically severe dry eye, phthisis or suspicion of phthisis, ocular hypotension

132 of less than 6 mmHg or ocular hypertension of more than 25 mmHg, aphakia, significant iris
133 defect that could compromise intraoperative anterior chamber stability, a history of corneal
134 refractive surgery, glaucoma shunts (e.g., Ahmed valve), neurotrophic keratopathy, a history of
135 persistent corneal erosion, difficulties with epithelial growth (re-epithelization), or participation
136 in another investigational study within the past 60 days.

137

138 Device Description:

139 The EndoArt® implant is a transparent, foldable, and hydrophilic device composed of a copolymer
140 of hydroxyethyl methacrylate and methyl methacrylate. This material is commonly used in the
141 manufacturing of IOLs. The implants used in this study had a diameter ranging from 5-6.5 mm, a
142 radius of curvature of 6.8 mm, a thickness of 50 µm, and no optical power.

143

144 Implantation Procedure:

145 The implantation of EndoArt® is very similar to that of DSAEK. A peripheral corneal incision of
146 approximately 2.4 mm was made to insert the device. The endothelial cell layer was either left
147 untouched or removed (Descemetorhexis) at the physician's discretion. The folded EndoArt®
148 device was placed into the anterior chamber through a peripheral corneal incision using an off-
149 the-shelf injector or spatula. Once inside the eye, the device was allowed to unfold and was
150 positioned centrally adjacent to the posterior surface of the cornea. To secure the device onto
151 the posterior corneal surface, either an air bubble was introduced, or, through off-label

152 applications, injections of 20% sulfur hexafluoride (SF6) gas or 10% perfluoropropane (C3F8) gas
153 were made into the anterior chamber, and according to the physician's discretion, a temporary
154 fixating suture was placed at 12 o'clock. Immediately after the procedure, the subject was placed
155 supine and faced up for 2.5-4 hours. The subject was either discharged after the procedure or
156 hospitalized at the physician's discretion.

157

158 Visits and procedure:

159 Each participant underwent a comprehensive baseline evaluation, which included a BCDVA
160 assessment using the ETDRS visual acuity score, pachymetry measurement of CCT by Optical
161 Coherence Tomography (OCT), anterior and posterior segment examination using a slit lamp,
162 endothelial cell count (if feasible), intraocular pressure (IOP) measurement (Goldman
163 applanator), pain assessment using a Visual Analogue Scale (VAS, 0-100) and color photography
164 of the cornea. Corneal clarity was evaluated using a slit lamp and graded as 0 (clear), 1 (clear iris
165 details), 2 (obscured iris details), 3 (pupil barely visible), or 4 (pupil or iris details not visible).
166 Ophthalmic assessments were conducted on days 1, 7, and 14, followed by assessments every 2
167 weeks for up to 3 months, monthly assessments for the first 6 months, and then every other
168 month for up to 1 year after the procedure. Adverse events were monitored throughout the
169 entire duration of the study period.

170

171 Statistical analysis

172 The Wilcoxon signed rank test was used to determine statistically significant changes from
173 baseline. Calculations were performed using the stats.wilcoxon function in scipy library in
174 Python.

175 Results:

176 Twenty-four (24) participants were enrolled, and 17 (71%) completed the one-year follow-up
177 (Table 1). Table 2 summarizes the characteristics of the study population. The mean age of the
178 participants was 69.8±9.6 years, and 41.7% of the participants were female. All subjects had a
179 history of cataract extraction, and five had prior corneal surgeries. More than 30% of the subjects
180 had a posterior segment comorbidity.

181

182 TABLE 1 STUDY COMPLETION AND REASONS FOR DROPOUT

Group		Number	Remarks
Enrolled		24	
Completed 1 year of follow up		17	
Dropout	Implant did not attach	5	Descemetorhexis was not performed
	Other	2	<ul style="list-style-type: none">• Procedural failure; non-device related IOL dislocation.• Subject lost to follow up.

183

184

185

Characteristic	
Age (years), Mean \pm SD (range)	69.8 \pm 9.6 (54 – 86)
Female gender, n (%)	10 (41.7)
Ophthalmic history, n (%)	
Cataract extraction	24 (100.0)
ACIOL	1 (4.2)
Glaucoma	4 (16.7)
Previous glaucoma filtering surgery	2 (8.3)
Previous retinal detachment	3 (12.5)
Vitreous or retinal disease	5 (20.8)
Prior corneal surgery	
DMEK	2 (8.3)
DSAEK	2 (8.3)
DSO	1 (4.2)

187 ACIOL (Anterior Chamber Intraocular Lens), DSAEK (Descemet Stripping Automated Endothelial
188 Keratoplasty), (DMEK) Descemet Membrane Endothelial Keratoplasty, DSO (Descemet Stripping
189 Only)

190

191 Primary Safety Results

192 Throughout the follow-up period, no serious device-related adverse events were reported
193 (n=24), nor were any chronic inflammatory reactions observed in the treated eyes. No device-
194 related irritation, infection, uncontrolled IOP, or corneal melting was observed. One (1)
195 procedure-related SAE was reported, where the EndoArt® was inverted and required
196 repositioning. One (1) subject demonstrated herpetic epithelial and stromal keratitis, with
197 melting and thinning, which healed with topical acyclovir and systemic steroids without EndoArt®
198 removal. Transient eye pain was reported in 6 patients (25%) mainly due to dry eye or transient
199 bullae. Four patients experienced perioperative IOP elevation, all occurring following gas bubble
200 injection. In three of these patients, paracentesis was necessary for resolution. Transient corneal
201 epithelial defects/ bullae were reported in 4 cases and treated with contact lenses (see Table 3).
202 Increase in lacrimation, dry eye, ptosis and macular oedema were each reported in one subject.

203 TABLE 3 ADVERSE EVENTS

Adverse event	Number of subjects, n (%)	Comments
---------------	------------------------------	----------

Eye pain	6 (25)	In two cases, the implant was not attached
Intraocular pressure increased	4 (16.7)	Perioperative due to gas bubble
Transient corneal epithelial defect/ bullae	4 (16.7)	
Ocular discomfort	2 (8.3)	
Conjunctivitis	2 (8.3)	

204

205 Re-bubbling Procedure

206 A re-bubbling procedure was performed when a complete or clinically significant partial
 207 detachment of the EndoArt® implant was identified. Throughout the trial, an average re-bubbling
 208 rate of 2.9 ± 2.0 procedures per subject was documented. During the study, an improved
 209 attachment technique was established, including an obligatory Descemetorhexis, a temporary
 210 fixation suture, and the utilization of long-lasting gas, resulting in no detachment or the necessity
 211 for re-bubbling in the final two patients.

212

213 First-In-Human (FIH) Dropout

214 Six (6) EndoArt® implants (25.0%) were explanted. In five (5) patients, the devices were explanted
 215 due to attachment failure despite repeated re-bubbling and replaced with DSAEK. In all those
 216 patients, Descemetorhexis was not performed. In one (1) patient, the IOL was dislocated during
 217 the procedure, which led to an inability to create an effective air bubble and was converted to

218 Penetrating Keratoplasty (PK). The removal of all devices was straightforward, without any
219 complications.

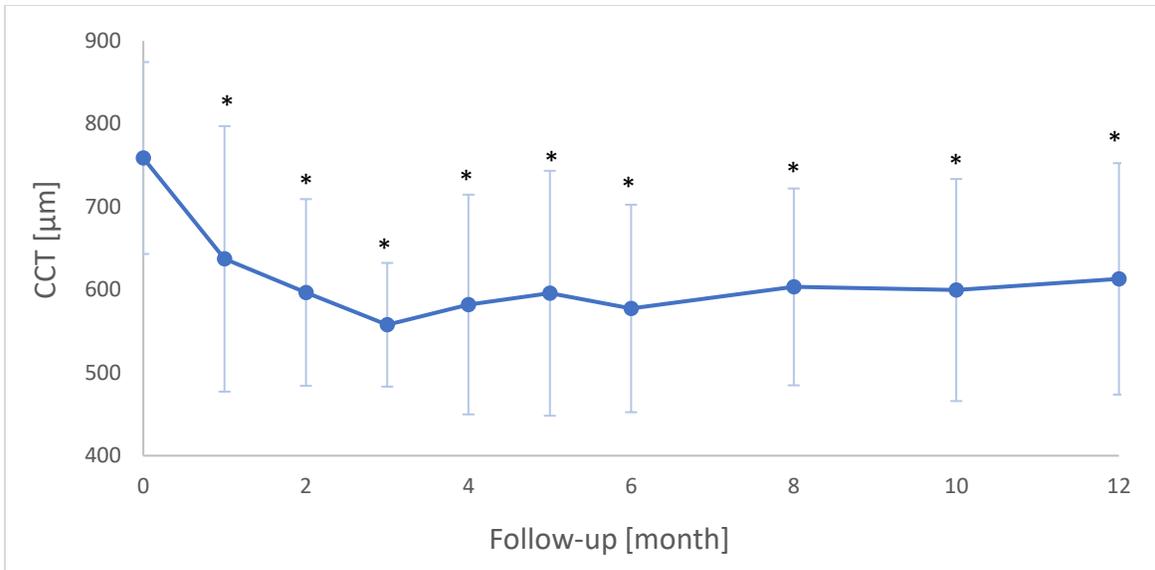
220

221 Secondary efficacy results

222 Central Corneal Thickness (CCT)

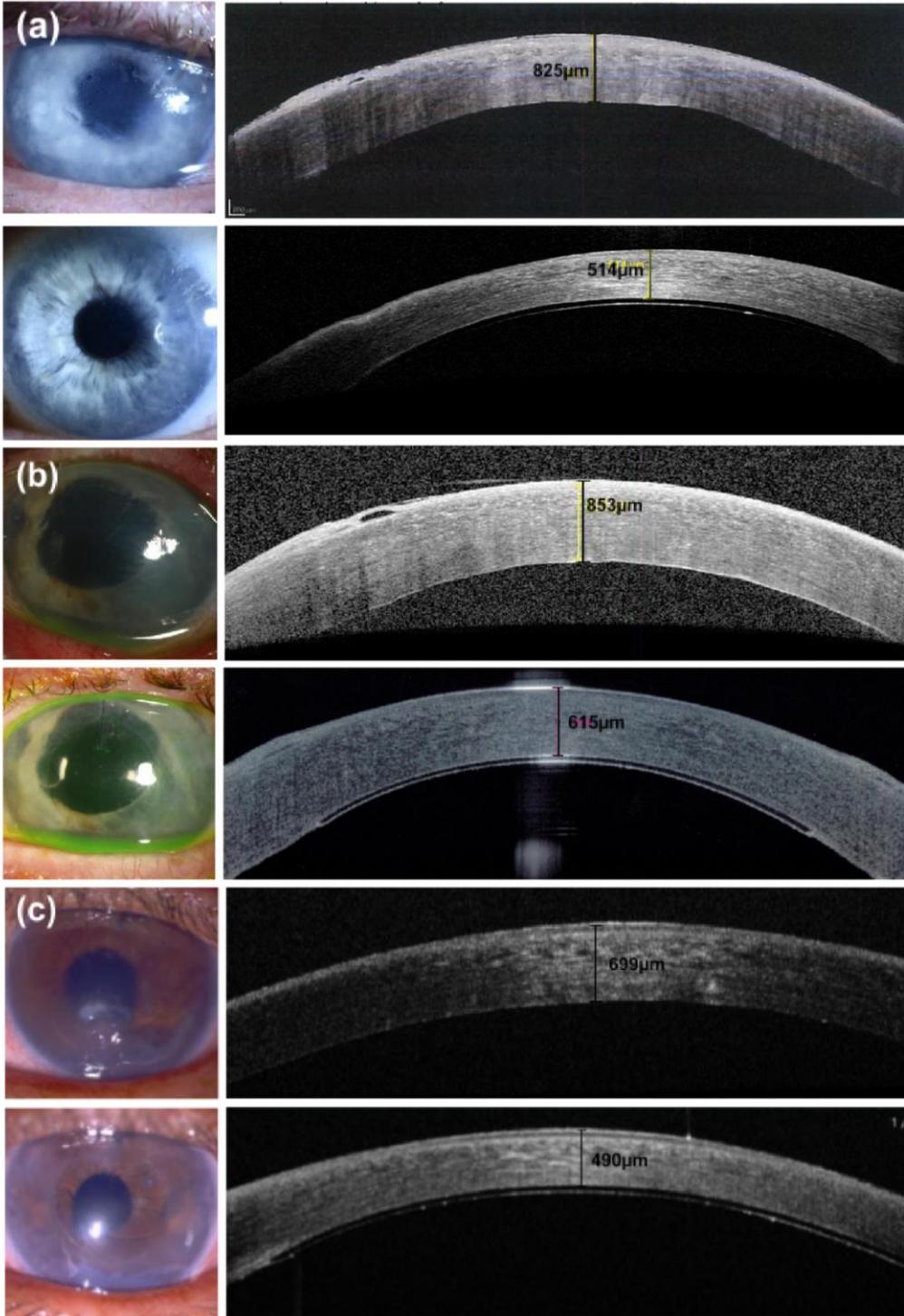
223 The CCT decreased from an average baseline measurement of $759 \pm 116 \mu\text{m}$ to $613 \pm 135 \mu\text{m}$
224 ($n=17$) at 12-months. Significant improvement was noted in the first month after implantation
225 (Figure 1) and remained stable throughout the follow-up. In four (4) patients, the CCT did not
226 show improvement. Among them, three (3) subjects faced insufficient implant attachment, while
227 one subject (1) subject experienced subepithelial fibrosis. Figure 2 illustrates the improvement
228 in CCT once EndoArt® is fully attached using OCT and slit-lamp images of three subjects at
229 baseline and 12-months post-implantation.

230



231

232 Figure 1: Central corneal thickness (CCT) after EndoArt® implantation. The mean \pm SD CCT over
 233 time is displayed. A significant improvement from the baseline CCT was observed at the 1-month
 234 follow-up, and the CCT remained stable throughout the 12-month follow-up (n=17). *p<0.05



235

236 Figure 2: Changes in Clarity and Central Corneal Thickness (CCT). Slit-lamp color photography and
 237 optical coherence tomography (OCT) images at baseline (upper images) and 12 months (lower

238 images) after EndoArt® implantation into the eye of (a) a 67-year-old male, pseudophakic,
239 myopic, after failed DSO; (b) an 80-year-old male, pseudophakic, after glaucoma filtering surgery;
240 and (c) a 60-year-old male, pseudophakic (ACIOL), with a macular scar.

241

242 Corneal Clarity

243 A significant improvement in central corneal clarity was observed within two weeks of surgery,
244 and the degree of improvement remained stable during the 12-month follow-up period. The
245 average clarity improved from 3.2 ± 0.6 at baseline to 1.1 ± 1.1 at the 12-month follow-up.

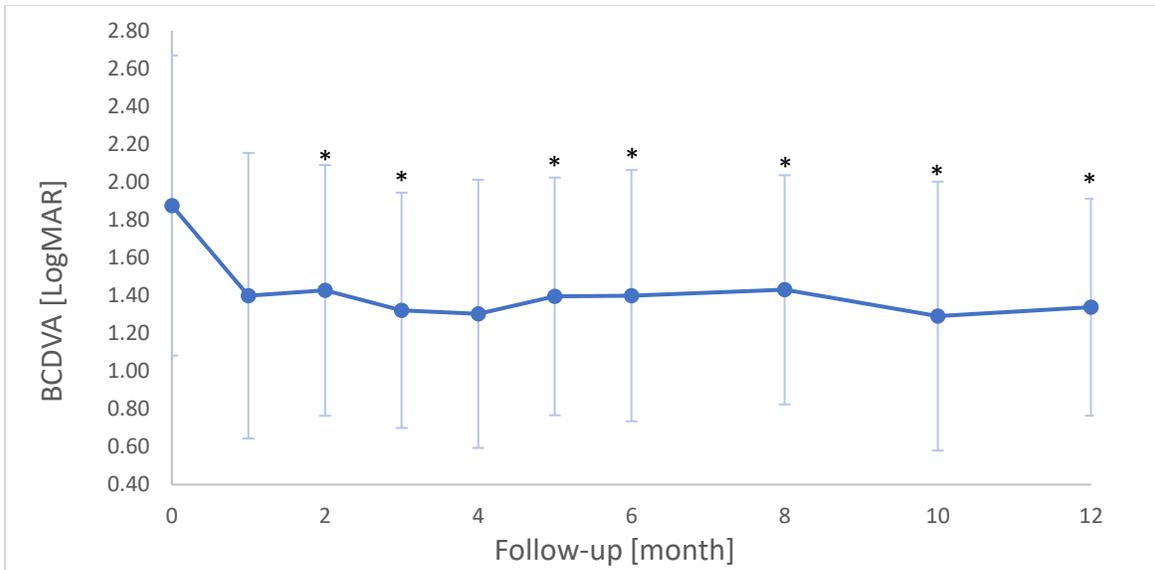
246

247 Best Corrected Distance Visual Acuity (BCDVA)

248 Of the 17 subjects who reached the 12-month follow-up assessment, two (2) had no vision due
249 to optic neuropathy and were therefore not assessed for visual acuity throughout the study.

250 Despite low visual potential in 10 of the remaining 15 subjects, attributed to ocular conditions
251 such as retinal detachment, macular scarring, amblyopia, and cystoid macular edema, there was
252 a significant improvement in average visual acuity (VA). VA improved from a baseline LogMAR
253 score of 1.88 ± 0.79 to 1.34 ± 0.57 at 12-month follow-up (Figure 3). Notably, 60% of the patients
254 (9 out of 15) improved at least three lines of ETDRS. The most remarkable improvement in VA
255 was from FC to 0.6 logMAR (6/24).

256



257

258 Figure 3: Best-Corrected Distance Visual Acuity (BCDVA) after EndoArt® implantation in subjects
 259 with low to normal visual potential. The mean \pm SD BCDVA over time after EndoArt® implantation
 260 is displayed. A clinically significant improvement from baseline was observed (n=15). *p<0.05

261

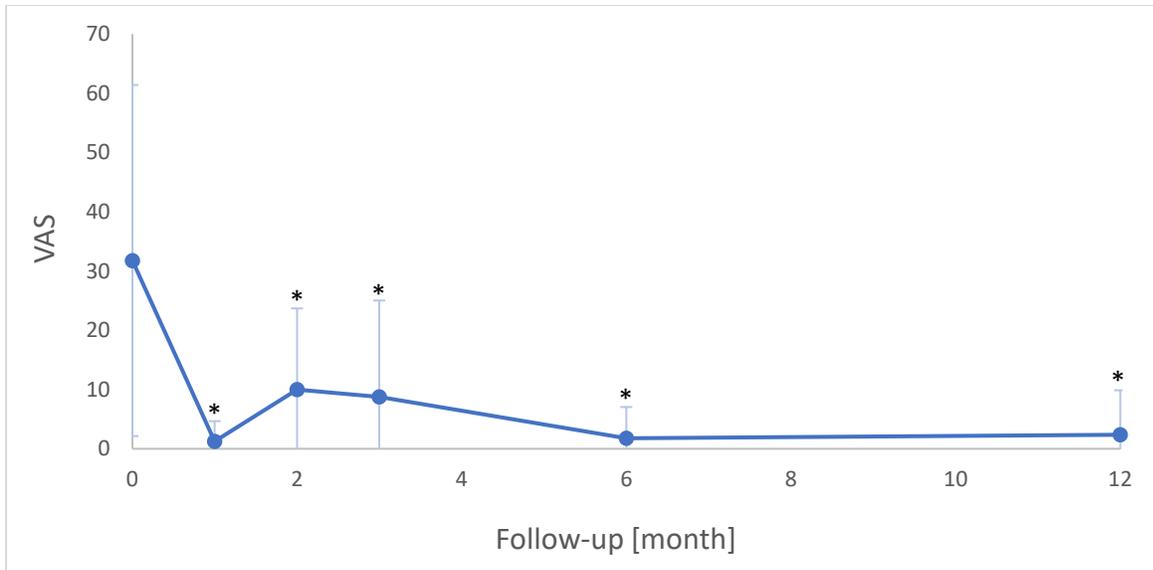
262 Pain Score

263 The average VAS (0-100) score significantly decreased from 32 ± 30 at baseline to 2 ± 8 12 months
 264 after EndoArt® implantation (Figure 4). All subjects who complained of pain (VAS \neq 0) at baseline
 265 (11 out of 17) experienced pain relief.

266

267

268



269

270 Figure 4: Pain score in Visual Analogue Scale (VAS) after EndoArt® implantation. The mean ± SD
271 pain score was measured using a visual analogue scale. Significant pain relief was noted at all
272 time points (n=17). *p<0.05

273

274 Discussion:

275 The FIH study proved the concept of reducing corneal edema through a barrier mechanism rather
276 than solely relying on endothelial function. As the study progressed, it became apparent that the
277 performance of EndoArt® was closely tied to its attachment quality to the posterior cornea.
278 Factors influencing this attachment, such as the omission of Descemetorhexis, were scrutinized
279 during the study. Indeed, in five (5) cases where Descemetorhexis was not performed, the
280 implant could not achieve attachment and had to be explanted. Surgical steps promoting
281 attachment were identified and consolidated into a protocol. This protocol included a 7.0-7.5 mm
282 Descemetorhexis, a single fixation suture, and 10% C₃F₈ gas for all implantations. Integrating
283 these steps into the EndoArt® implantation technique showed a trend toward minimizing the
284 need for re-bubbling, ultimately resulting in successful attachment in the last two patients
285 without requiring additional re-bubbling. Further details on implementing this modified
286 implantation technique will be provided in upcoming publications of a more extensive cohort
287 study.

288 The main concerns surrounding potential adverse events associated with keratoprotheses were
289 corneal melting and perforation, both consequences of insufficient corneal nutrition, however,
290 none of the 24 implanted subjects presented any signs of corneal nutrients depletion. Concerns
291 regarding uncontrolled inflammation and severe infection were also refuted, as none of the
292 subjects exhibited a prolonged inflammatory response. No serious device-related adverse events
293 were reported during the 12-months follow-up. The main adverse events involved ocular pain
294 and discomfort, all resolving during the follow-up period, as well as elevated IOP resulting from

295 gas bubble injection. The latter required paracentesis to relieve the high IOP in 3 cases. To
296 mitigate the risk of post-operative pupillary block, iridectomy was introduced as a mandatory
297 procedural step.

298 Over the 12-month follow-up period, a clinically significant decrease in the average CCT was
299 observed in the 17 subjects who completed the study. This decrease in CCT correlated with
300 improved central corneal clarity, as anticipated. As corneal clarity improved, VA enhanced, even
301 among subjects deemed to have low visual potential due to comorbidities. Notably, despite most
302 patients having low visual potential, 60% of all patients exhibited improvements of at least 3 lines
303 in visual acuity at the 12-month follow-up, with the best 12-month VA reaching 0.6 logMAR
304 (6/24).

305 Similar results were reported in another case series²⁷ involving five (5) patients with prior EK
306 failures who were implanted with EndoArt®. Corneal clarity and VA showed improvement, with
307 the most significant 6-month improvement in VA recorded from 1.3 logMAR at baseline to 0.2
308 logMAR (6/9.5). Furthermore, all subjects who reported pain at baseline experienced substantial
309 pain relief after EndoArt® implantation. Importantly, no significant complications, such as corneal
310 melting, chronic inflammation, or related infections, were observed during the follow-up period.

311 It is important to acknowledge the study's limitations, including the evolving method of EndoArt®
312 implantation over the trial period and difficulties with the early learning curve. In the future, the
313 results of a more extended follow-up period should be reported.

314 This FIH study provides evidence supporting the concept that EndoArt® may act as a passive
315 barrier, effectively reducing corneal edema and enhancing vision while demonstrating a relatively

316 safe profile with no device-related SAEs. The reported outcomes highlight its potential utility in
317 treating chronic corneal edema, particularly in high-risk patients with a history of graft rejection,
318 for which the non-rejection nature of EndoArt® is a key feature. Furthermore, EndoArt® may be
319 an available, ready-to-use option in geographic regions with a limited supply of donor corneas.
320 The observed detachment rate, possibly due to the initial learning curve, requires attention for
321 improvement. A more extensive follow-up period and larger cohort are essential to ascertain the
322 precise role of EndoArt® as a therapeutic tool in managing patients with corneal edema.

323

324

325

326 Data availability:

327 The datasets analyzed during the current study are not publicly available but are available from
328 the corresponding author upon reasonable request.

329

330 Competing interests:

331 The authors declare that they have no competing interests.

332

333 Authors' contributions:

334 OD is the inventor of EndoArt® and co-founder of EyeYon Medical. OD, EG, AL, and MD analyzed
335 and interpreted the EndoArt® FIH trial outcomes and wrote the manuscript. ALM is the co-
336 founder of EyeYon Medical. ALM contributed to the writing of the manuscript. RGL and GUA
337 participated in the EndoArt® FIH trial and contributed significantly to developing the implantation
338 technique. All authors have read and approved the final manuscript.

339

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345 David Varssano for participating.

346

347 List of Abbreviations:

SAE	Serious Adverse Event
CCT	Central Corneal Thickness
BCDVA	Best-Corrected Distance Visual Acuity
ETDRS	Early Treatment Diabetic Retinopathy Study
FIH	First-In-Human
EK	Endothelial Keratoplasty
DSAEK	Descemet Stripping Automated Endothelial Keratoplasty
DMEK	Descemet Membrane Endothelial Keratoplasty
IRIS	Intelligent Research in Sight
VA	Visual Acuity
ACIOL	Anterior Chamber Intraocular Lens
IOL	Intraocular Lens
OCT	Optical Coherence Tomography
IOP	Intraocular Pressure
VAS	Visual Analogue Scale
DSO	Descemet Stripping Only
PK	Penetrating Keratoplasty

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List of Figures:

Figure 1: Central corneal thickness (CCT) after EndoArt® implantation. The mean ± SD CCT over time is displayed. A significant improvement from the baseline CCT was observed at the 1-month follow-up, and the CCT remained stable throughout the 12-month follow-up (n=17). *p<0.05..... 16

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